

On Direct Distribution Matching for Adapting Segmentation Networks

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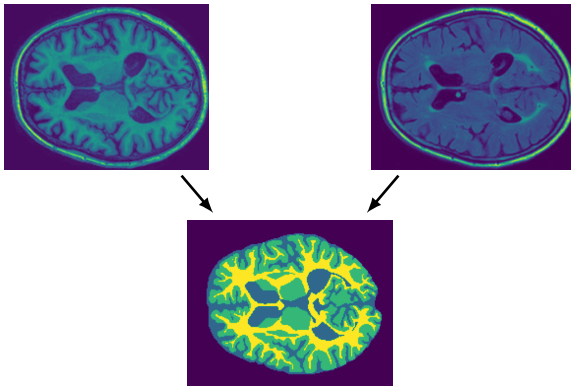
Domain Adaptation in Segmentation Networks

- Source domain images X ; ground truth labels Y
- A segmentation function f is trained on labeled source data $\mathcal{L} = \{(X_i, Y_i)\}_{i=1, \dots, n}$
- Images X' from a different, target domain:
 - taken with a different camera,
 - taken with a different MR/CT/X-ray machine, ...
- $f(X') \neq Y'$
- Domain Adaptation (DA): Obtain f' with good performance on X' , given \mathcal{L} and **unlabeled** pairs of source/target domain images $\mathcal{U} = \{(X_{n+1}, X'_{n+1}), \dots, (X_{n+m}, X'_{n+m})\}$

- Previous work dominated by adversarial approaches (Goodfellow et al. (2014))
 - Y.-H. Tsai et al. (2018). “Learning to adapt structured output space for semantic segmentation”. In: *Computer Vision and Pattern Recognition (CVPR)*
- Adversary can operate at output (segmentation) level
- Or image alignment at pixel/intermediate level:
 - Transform the source images into the style of the target images
 - Then train the segmentation network on **artificial** target images
 - Downside: only work well on narrow shifts between source and target domain

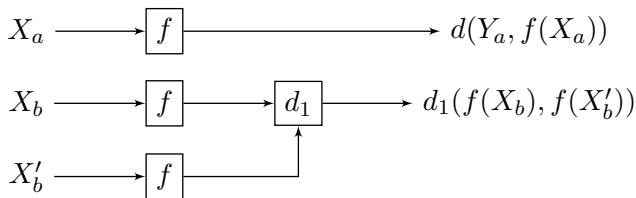
Domain Adaptation for Medical Images

- Possibility to obtain images of the same patient with different imaging methods (machines/protocols/cameras. . .)
⇒ Gap in appearance, but identical spacial layout



Proposed Approach

- **Goal:** Training one segmentation function f that works on both source and target domain
- **Idea:** Use \mathcal{U} to enforce $f(X) \approx f(X')$



- Utilize (C)NN architecture: f_θ with parameter θ
- **Loss:**

$$\mathcal{F}(\theta) = \sum_{i=1}^n d(Y_i, f_\theta(X_i)) + \lambda \sum_{i=n+1}^{n+m} d_1(f_\theta(X_i), f_\theta(X'_i))$$

- **Choices:** f_θ , d_1 , d , λ

Segmentation Network:

- f_θ : slightly modified **U-Net** (Ronneberger, Fischer, and Brox, 2015)

Datasets

- Human brain **MR images**
 - iSEG challenge dataset (Wang et al., 2019)
 - MRBrainS2013 challenge dataset (Mendrik et al., 2015)
- Segmentation in 3 classes: GM, WM, CSF
- X, X' : Aligned T1/T2(-FLAIR) scans of the same patient
- d, d_1 : cross entropy loss
- Three runs for cross-validation
- Figure of merit: average DICE over all three classes

- **Oracle:** U-Net network trained on target domain
- **No Adaptation:** U-Net network trained on source domain only
- **AdaptSegNet:** (Tsai et al., 2018) with U-Net segmentation net.

Targ.	Oracle	No adaptation	AdaptSegNet	Proposed
T2*	77.35 \pm 1.35	38.58 \pm 1.14	56.62 \pm 8.02	76.10 \pm 0.45
T1*	84.71 \pm 0.98	20.25 \pm 3.54	73.22 \pm 2.16	82.43 \pm 0.50
T2 [†]	76.89 \pm 0.67	38.70 \pm 10.46	63.37 \pm 6.25	74.17 \pm 0.78
T1 [†]	82.28 \pm 0.88	66.26 \pm 0.53	70.11 \pm 3.00	77.89 \pm 1.15

- Asymmetry between T1 \rightarrow T2 (harder) and T2 \rightarrow T1 (easier) (also noted by Dou et al., 2018)

*MRBrainS 2013

[†]iSEG






Domain adaptation in semantic segmentation of MR images

- Additional structure in data (e.g. alignment) should be utilized!

In the paper:

- **Stability** during training
- Violation of **alignment** assumption
- Impact of distance function d_1 and Lagrangian λ

References I

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